# Image Reconstruction in Computed Tomography From deterministic to probabilistic methods

Ali Mohammad-Djafari

Groupe Problèmes Inverses Laboratoire des Signaux et Systèmes UMR 8506 CNRS - SUPELEC - Univ Paris Sud 11 Supélec, Plateau de Moulon, 91192 Gif-sur-Yvette, FRANCE.

djafari@lss.supelec.fr
http://djafari.free.fr
http://www.lss.supelec.fr

European School of Medical Physics, Oct.-Nov. 2011

< 日 > < 同 > < 回 > < 回 > < 回 > <

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 1/56

# Content

- Seeing outside of a body: Image restoration
- Seeing inside of a body: Image reconstruction
- Computed Tomography: Different imaging systems

▲ 同 ▶ ▲ 国 ▶ ▲ 国 ▶ → 国

- Common inverse problem formulation
- Analytical Methods
- Algebraic Deterministic Methods
- Probabilistic Methods
- Bayesian approach
- Examples and case studies
- Questions and Discussion

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 2/56

Seeing outside of a body: Making an image with a camera, a microscope or a telescope

- ▶ f(x, y) real scene
- ▶ g(x, y) observed image
- ► Forward model: Convolution



$$g(x,y) = \iint f(x',y') h(x-x',y-y') dx' dy' + \epsilon(x,y)$$

h(x, y): Point Spread Function (PSF) of the imaging system

Inverse problem: Image restoration

Given the forward model  $\mathcal{H}$  (PSF h(x, y))) and a set of data  $g(x_i, y_i), i = 1, \dots, M$ find f(x, y)

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 3/56

# Making an image with an unfocused camera

Forward model: 2D Convolution

$$g(x,y) = \iint f(x',y') h(x-x',y-y') dx' dy' + \epsilon(x,y)$$



Inversion: Deconvolution



A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 4



Image: A mathematical states and a mathem

4/56

# Different ways to see inside of a body



・ロト ・ 一 ト ・ ヨ ト ・ 日 ト

3

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 5/56

# Seeing inside of a body: Computed Tomography

- f(x, y) a section of a real 3D body f(x, y, z)
- $g_{\phi}(r)$  a line of observed radiographe  $g_{\phi}(r, z)$
- Forward model:

Line integrals or Radon Transform

$$g_{\phi}(r) = \int_{L_{r,\phi}} f(x, y) \, dl + \epsilon_{\phi}(r)$$
  
= 
$$\iint f(x, y) \, \delta(r - x \cos \phi - y \sin \phi) \, dx \, dy + \epsilon_{\phi}(r)$$

#### Inverse problem: Image reconstruction

Given the forward model  $\mathcal{H}$  (Radon Transform) and a set of data  $g_{\phi_i}(r), i = 1, \cdots, M$ find f(x, y)

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 6/56





<ロ> < ()</p>

# 2D and 3D Computed Tomography



A. Mohammad-Diafari. ISIP 2012. Julv23-28, 2012. 7/56

・ロト ・聞ト ・ヨト ・ヨト

# Microwave or ultrasound imaging

Mesaurs: diffracted wave by the object  $\phi_d(\mathbf{r}_i)$ Unknown quantity:  $f(\mathbf{r}) = k_0^2(n^2(\mathbf{r}) - 1)$ Intermediate quantity :  $\phi(\mathbf{r})$ 

$$\phi_{d}(\mathbf{r}_{i}) = \iint_{D} G_{m}(\mathbf{r}_{i}, \mathbf{r}')\phi(\mathbf{r}') f(\mathbf{r}') d\mathbf{r}', \ \mathbf{r}_{i} \in S$$
  
$$\phi(\mathbf{r}) = \phi_{0}(\mathbf{r}) + \iint_{D} G_{o}(\mathbf{r}, \mathbf{r}')\phi(\mathbf{r}') f(\mathbf{r}') d\mathbf{r}', \ \mathbf{r} \in S$$

Born approximation  $(\phi(\mathbf{r}') \simeq \phi_0(\mathbf{r}'))$  ):  $\phi_d(\mathbf{r}_i) = \iint_D G_m(\mathbf{r}_i, \mathbf{r}')\phi_0(\mathbf{r}') f(\mathbf{r}') d\mathbf{r}', \ \mathbf{r}_i \in S$ 

**Discretization**:

$$\begin{cases} \phi_d = \mathbf{G}_m \mathbf{F} \phi \\ \phi = \phi_0 + \mathbf{G}_o \mathbf{F} \phi \end{cases} \begin{cases} \phi_d = \mathbf{H}(\mathbf{f}) \\ \text{with } \mathbf{F} = \text{diag}(\mathbf{f}) \\ \mathbf{H}(\mathbf{f}) = \mathbf{G}_m \mathbf{F} (\mathbf{I} - \mathbf{G}_o \mathbf{F})^{-1} \end{cases}$$

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 8/56



Fourier Synthesis in X ray Tomography



Fourier Synthesis in X ray tomography

$$F(\omega_x, \omega_y) = \iint f(x, y) \exp \{-j\omega_x x, \omega_y y\} \, \mathrm{d}x \, \mathrm{d}y$$



A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

10/56

< □ > < 同 >

# Fourier Synthesis in Diffraction tomography



(日)

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 11/56

# Fourier Synthesis in Diffraction tomography

$$F(\omega_x, \omega_y) = \iint f(x, y) \exp \{-j\omega_x x, \omega_y y\} \, \mathrm{d}x \, \mathrm{d}y$$



A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

12/56

A B > 
 A
 B > 
 A
 B
 A
 B
 A
 B
 A
 A
 B
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A
 A

# Fourier Synthesis in different imaging systems



A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 13/56

Invers Problems: other examples and applications

- X ray, Gamma ray Computed Tomography (CT)
- Microwave and ultrasound tomography
- Positron emission tomography (PET)
- Magnetic resonance imaging (MRI)
- Photoacoustic imaging
- Radio astronomy
- Geophysical imaging
- Non Destructive Evaluation (NDE) and Testing (NDT) techniques in industry

- 4 同 6 4 日 6 4 日 6 日 日

- Hyperspectral imaging
- Earth observation methods (Radar, SAR, IR, ...)
- Survey and tracking in security systems

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 14/56

# Computed tomography (CT)

#### A Multislice CT Scanner





$$g(s_i) = \int_{L_i} f(\mathbf{r}) \, \mathrm{d}l_i + \epsilon(s_i)$$
  
Discretization  
$$\mathbf{g} = \mathbf{H}\mathbf{f} + \epsilon$$

A 10

A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

15/56

# Magnetic resonance imaging (MRI)

Nuclear magnetic resonance imaging (NMRI), Para-sagittal MRI of the head



 $\mathcal{O} \mathcal{Q} \mathcal{O}$ 

# X ray Tomography





A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

17/56

< □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > <



# Filtered Backprojection method

$$f(x,y) = \left(-\frac{1}{2\pi^2}\right) \int_0^{\pi} \int_{-\infty}^{+\infty} \frac{\frac{\partial}{\partial r}g(r,\phi)}{(r-x\cos\phi - y\sin\phi)} \, \mathrm{d}r \, \mathrm{d}\phi$$

Derivation 
$$\mathcal{D}$$
:  $\overline{g}(r,\phi) = \frac{\partial g(r,\phi)}{\partial r}$   
Hilbert Transform $\mathcal{H}$ :  $g_1(r',\phi) = \frac{1}{\pi} \int_0^\infty \frac{\overline{g}(r,\phi)}{(r-r')} dr$   
Backprojection  $\mathcal{B}$ :  $f(x,y) = \frac{1}{2\pi} \int_0^\pi g_1(r' = x \cos \phi + y \sin \phi, \phi) d\phi$ 

$$f(x,y) = \mathcal{B} \mathcal{H} \mathcal{D} g(r,\phi) = \mathcal{B} \mathcal{F}_1^{-1} |\Omega| \mathcal{F}_1 g(r,\phi)$$

• Backprojection of filtered projections:



# Limitations : Limited angle or noisy data



- Limited angle or noisy data
- Accounting for detector size
- Other measurement geometries: fan beam, ...

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 20/56

# CT as a linear inverse problem



► g, f and H are huge dimensional A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 21/56

# Algebraic methods: Discretization





 $\mathbf{g} = \mathbf{H}\mathbf{f} + \boldsymbol{\epsilon}$ 

A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

2, 22/56

・ロト・西ト・西ト・西・ うんの

# Inversion: Deterministic methods Data matching

Observation model

$$g_i = h_i(\mathbf{f}) + \epsilon_i, \quad i = 1, \dots, M \longrightarrow \mathbf{g} = \mathbf{H}(\mathbf{f}) + \epsilon$$

► Misatch between data and output of the model ∆(g, H(f))

$$\widehat{\mathbf{f}} = rg \min \left\{ \Delta(\mathbf{g}, \mathbf{H}(\mathbf{f})) 
ight\}$$

Examples:

- LS 
$$\Delta(\mathbf{g}, \mathbf{H}(\mathbf{f})) = \|\mathbf{g} - \mathbf{H}(\mathbf{f})\|^2 = \sum_i |g_i - h_i(\mathbf{f})|^2$$

$$-L_p \qquad \Delta(\mathbf{g},\mathbf{H}(\mathbf{f})) = \|\mathbf{g}-\mathbf{H}(\mathbf{f})\|^p = \sum_i |g_i - h_i(\mathbf{f})|^p, \ 1$$

$$- \mathsf{KL} \qquad \Delta(\mathbf{g}, \mathbf{H}(\mathbf{f})) = \sum_{i} g_{i} \ln \frac{g_{i}}{h_{i}(\mathbf{f})}$$

 In general, does not give satisfactory results for inverse problems.

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 23/56

# Deterministic Inversion Algorithms

Least Squares Based Methods

$$\widehat{\mathbf{f}} = \arg\min_{\mathbf{f}} \{ J(\mathbf{f}) \} \quad \text{with} \quad J(\mathbf{f}) = \|\mathbf{g} - \mathbf{H}\mathbf{f}\|^2$$

$$\nabla J(\mathbf{f}) = -2\mathbf{H}^t(\mathbf{g} - \mathbf{H}\mathbf{f})$$

・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・
 ・

Gradient based algorithms:

Initialize: f<sup>(0)</sup>

► Iterate: 
$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} - \alpha \nabla J(\mathbf{f}^{(k)})$$

At each iteration:  $\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \alpha \mathbf{H}^t \left( \mathbf{g} - \mathbf{H} \mathbf{f}^{(k)} \right)$ we have to do the following operations:

- Compute  $\hat{\mathbf{g}} = \mathbf{H}\mathbf{f}$  (Forward projection)
- Compute  $\delta \mathbf{g} = \mathbf{g} \widehat{\mathbf{g}}$  (Error or residual)
- Distribute  $\delta \mathbf{f} = \mathbf{H}^t \delta \mathbf{g}$  (Backprojection of error)
- Update  $\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \delta \mathbf{f}$

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 24/56

# Gradient based algorithms

Operations at each iteration:  $\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \alpha \mathbf{H}^t \left( \mathbf{g} - \mathbf{H} \mathbf{f}^{(k)} \right)$ 

- Compute  $\widehat{\mathbf{g}} = \mathbf{H}\mathbf{f}$  (Forward projection)
- Compute  $\delta \mathbf{g} = \mathbf{g} \widehat{\mathbf{g}}$  (Error or residual)
- Distribute  $\delta \mathbf{f} = \mathbf{H}^t \delta \mathbf{g}$  (Backprojection of error)

• Update 
$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \delta \mathbf{f}$$



ヘロト ヘヨト ヘヨト

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 25/56

# Gradient based algorithms

Fixed step gradient:

$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \alpha \mathbf{H}^t \left( \mathbf{g} - \mathbf{H} \mathbf{f}^{(k)} \right)$$

Steepest descent gradient:

$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \alpha^{(k)} \mathbf{H}^t \left( \mathbf{g} - \mathbf{H} \mathbf{f}^{(k)} \right)$$

with  $\alpha^{(k)} = \arg \min_{\alpha} \{ J(\mathbf{f} + \alpha \delta \mathbf{f}) \}$ 

Conjugate Gradient

$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \alpha^{(k)} \mathbf{d}^{(k)}$$

The successive directions  $\mathbf{d}^{(k)}$  have to be conjugate to each other.

A. Mohammad-Djafari, ISIP 2012, Julv23-28, 2012.

26/56

◆□▶ ◆□▶ ▲□▶ ▲□▶ ▲□ ◆ ●

# Algebraic Reconstruction Techniques

Main idea: Use the data as they arrive

$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \alpha^{(k)} [\mathbf{H}^t]_{i*} \left( g_i - [\mathbf{H}\mathbf{f}^{(k)}]_i \right)$$

which can also be written as:

$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \frac{\left(g_i - [\mathbf{H}\mathbf{f}^{(k)}]_i\right)}{\mathbf{h}_{i*}^t \mathbf{h}_{i*}} \mathbf{h}_{i*}^t$$
$$= \mathbf{f}^{(k)} + \sum_i \frac{\left(g_i - \sum_j H_{ij} f_j^{(k)}\right)}{\sum_i H_{ij}^2} H_{ij}$$

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012,

27/56

# Algebraic Reconstruction Techniques

Use the data as they arrive

$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \frac{\left(g_i - [\mathbf{H}\mathbf{f}^{(k)}]_i\right)}{\mathbf{h}_{i*}^t \mathbf{h}_{i*}} \mathbf{h}_{i*}^t$$
$$= \mathbf{f}^{(k)} + \sum_i \frac{\left(g_i - \sum_j H_{ij} f_j^{(k)}\right)}{\sum_i H_{ij}^2} H_{ij}$$

Update each pixel at each time

$$f_{j}^{(k+1)} = f_{j}^{(k)} + rac{\left(g_{i} - \sum_{j} H_{ij} f_{j}^{(k)}
ight)}{\sum_{i} H_{ij}^{2}} H_{ij}$$

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012,

28/56

# Algebraic Reconstruction Techniques (ART)

$$\mathbf{f}^{(k+1)} = \mathbf{f}^{(k)} + \sum_{i} \frac{\left(g_{i} - \sum_{j} H_{ij} f_{j}^{(k)}\right)}{\sum_{i} H_{ij}^{2}} H_{ij}$$

or

$$f_{j}^{(k+1)} = f_{j}^{(k)} + \frac{\left(g_{i} - \sum_{j} H_{ij} f_{j}^{(k)}\right)}{\sum_{i} H_{ij}^{2}} H_{ij}$$



A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 29/56

(日)

Algebraic Reconstruction using KL distance

• 
$$\widehat{\mathbf{f}} = \arg\min_{\mathbf{f}} \{J(\mathbf{f})\}$$
 with  $J(\mathbf{f}) = \sum_{i} g_{i} \ln \frac{g_{i}}{\sum_{j} H_{ij} f_{j}}$   
 $f_{j}^{(k+1)} = \frac{f_{j}^{(k)}}{\sum_{i} H_{ij}} \sum_{i} H_{ij} \frac{g_{i}}{\sum_{j} H_{ij} f_{j}^{(k)}}$ 

Interestingly, this is the OSEM (Ordered subset Expectation-Maximization) algorithm which is based on Maximum Likelihood and proposed first by Shepp & Vardi.



# Inversion: Regularization theory

Inverse problems = III posed problems  $\longrightarrow$  Need for prior information

Functional space (Tikhonov):

$$g = \mathcal{H}(f) + \epsilon \longrightarrow J(f) = ||g - \mathcal{H}(f)||_2^2 + \lambda ||\mathcal{D}f||_2^2$$

Finite dimensional space (Philips & Towmey):  $\mathbf{g} = \mathbf{H}(\mathbf{f}) + \boldsymbol{\epsilon}$ 

- Minimum norme LS (MNLS):  $J(\mathbf{f}) = ||\mathbf{g} \mathbf{H}(\mathbf{f})||^2 + \lambda ||\mathbf{f}||^2$  $J(\mathbf{f}) = ||\mathbf{g} - \mathbf{H}(\mathbf{f})||^2 + \lambda ||\mathbf{D}\mathbf{f}||^2$
- Classical regularization:
- More general regularization:

$$J(\mathbf{f}) = \mathcal{Q}(\mathbf{g} - \mathbf{H}(\mathbf{f})) + \lambda \Omega(\mathbf{D}\mathbf{f})$$

or

$$J(\mathbf{f}) = \Delta_1(\mathbf{g}, \mathbf{H}(\mathbf{f})) + \lambda \Delta_2(\mathbf{f}, \mathbf{f}_0)$$

▲日▼▲□▼▲□▼▲□▼ □ ののの

# Limitations:

- Errors are considered implicitly white and Gaussian
- Limited prior information on the solution
- Lack of tools for the determination of the hyperparameters

Julv23-28, 2012. A. Mohammad-Djafari, ISIP 2012. 31/56 Bayesian estimation approach

$$\mathcal{M}$$
 :  $\mathbf{g} = \mathbf{H}\mathbf{f} + \boldsymbol{\epsilon}$ 

- Observation model  $\mathcal{M}$  + Hypothesis on the noise  $\epsilon \longrightarrow p(\mathbf{g}|\mathbf{f}; \mathcal{M}) = p_{\epsilon}(\mathbf{g} \mathbf{H}\mathbf{f})$ 
  - $P(\mathbf{z})$
- A priori information

$$p(\mathbf{f}|\mathcal{M})$$
$$p(\mathbf{f}|\mathbf{g};\mathcal{M}) = \frac{p(\mathbf{g}|\mathbf{f};\mathcal{M}) p(\mathbf{f}|\mathcal{M})}{p(\mathbf{g}|\mathcal{M})}$$

▲日▼▲□▼▲□▼▲□▼ □ ののの

## Link with regularization :

Bayes :

Maximum A Posteriori (MAP) :

$$\widehat{\mathbf{f}} = \arg \max_{\mathbf{f}} \{ p(\mathbf{f}|\mathbf{g}) \} = \arg \max_{\mathbf{f}} \{ p(\mathbf{g}|\mathbf{f}) \ p(\mathbf{f}) \}$$

$$= \arg \min_{\mathbf{f}} \{ -\ln p(\mathbf{g}|\mathbf{f}) - \ln p(\mathbf{f}) \}$$

with  $Q(\mathbf{g}, \mathbf{Hf}) = -\ln p(\mathbf{g}|\mathbf{f})$  and  $\lambda \Omega(\mathbf{f}) = -\ln p(\mathbf{f})$ But, Bayesian inference is not only limited to MAP

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 32/56

# Case of linear models and Gaussian priors $\mathbf{g} = \mathbf{H}\mathbf{f} + \boldsymbol{\epsilon}$

• Hypothesis on the noise:  $\boldsymbol{\epsilon} \sim \mathcal{N}(\mathbf{0}, \sigma_{\epsilon}^2 \mathbf{I})$ 

$$p(\mathbf{g}|\mathbf{f}) \propto \exp\left\{-\frac{1}{2\sigma_{\epsilon}^{2}}\|\mathbf{g} - \mathbf{H}\mathbf{f}\|^{2}
ight\}$$
  
Hypothesis on  $\mathbf{f} : \mathbf{f} \sim \mathcal{N}(\mathbf{0}, \sigma_{f}^{2}\mathbf{I})$ 

$$p(\mathbf{f}) \propto \exp\left\{-\frac{1}{2\sigma_f^2}\|\mathbf{f}\|^2\right\}$$

A posteriori:

►

$$p(\mathbf{f}|\mathbf{g}) \propto \exp\left\{-\frac{1}{2\sigma_{\epsilon}^{2}}\|\mathbf{g} - \mathbf{H}\mathbf{f}\|^{2} - \frac{1}{2\sigma_{f}^{2}}\|\mathbf{f}\|^{2}\right\}$$
  

$$\mathsf{MAP}: \quad \widehat{\mathbf{f}} = \arg\max_{\mathbf{f}} \left\{p(\mathbf{f}|\mathbf{g})\right\} = \arg\min_{\mathbf{f}} \left\{J(\mathbf{f})\right\}$$
with
$$J(\mathbf{f}) = \|\mathbf{g} - \mathbf{H}\mathbf{f}\|^{2} + \lambda \|\mathbf{f}\|^{2}, \quad \lambda = \frac{\sigma_{\epsilon}^{2}}{\sigma_{f}^{2}}$$

Advantage : characterization of the solution

$$\mathbf{f}|\mathbf{g} \sim \mathcal{N}(\mathbf{\widehat{f}}, \mathbf{\widehat{P}})$$
 with  $\mathbf{\widehat{f}} = \mathbf{\widehat{P}}\mathbf{H}^{t}\mathbf{g}$ ,  $\mathbf{\widehat{P}} = (\mathbf{H}^{t}\mathbf{H} + \lambda\mathbf{I})^{-1}$ 

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 33/56

MAP estimation with other priors:

$$\widehat{\mathbf{f}} = \arg\min_{\mathbf{f}} \{J(\mathbf{f})\} \text{ with } J(\mathbf{f}) = \|\mathbf{g} - \mathbf{H}\mathbf{f}\|^2 + \lambda \Omega(\mathbf{f})$$

Separable priors:

- Gaussian:  $p(f_j) \propto \exp\left\{-\alpha |f_j|^2\right\} \longrightarrow \Omega(\mathbf{f}) = \|\mathbf{f}\|^2 = \alpha \sum_j |f_j|^2$
- Gamma:  $p(f_j) \propto f_j^{\alpha} \exp\{-\beta f_j\} \longrightarrow \Omega(\mathbf{f}) = \alpha \sum_j \ln f_j + \beta f_j$
- ► Beta:  $p(f_j) \propto f_j^{\alpha} (1 - f_j)^{\beta} \longrightarrow \Omega(\mathbf{f}) = \alpha \sum_j \ln f_j + \beta \sum_j \ln(1 - f_j)$
- ► Generalized Gaussian:  $p(f_j) \propto \exp \{-\alpha |f_j|^p\}, \quad 1$

Markovian models:

$$p(f_j|\mathbf{f}) \propto \exp\left\{-\alpha \sum_{i \in N_j} \phi(f_j, f_i)\right\} \longrightarrow \quad \Omega(\mathbf{f}) = \alpha \sum_j \sum_{i \in N_j} \phi(f_j, f_i),$$

▲日▼▲□▼▲□▼▲□▼ □ ののの

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 34/56

# Main advantages of the Bayesian approach

- MAP = Regularization
- Posterior mean ? Marginal MAP ?
- More information in the posterior law than only its mode or its mean
- Meaning and tools for estimating hyper parameters
- Meaning and tools for model selection
- More specific and specialized priors, particularly through the hidden variables
- More computational tools:
  - Expectation-Maximization for computing the maximum likelihood parameters
  - MCMC for posterior exploration
  - Variational Bayes for analytical computation of the posterior marginals

► ...

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 35/56

# MAP estimation and Compressed Sensing

$$\begin{cases} \mathbf{g} = \mathbf{H}\mathbf{f} + \boldsymbol{\epsilon} \\ \mathbf{f} = \mathbf{W}\mathbf{z} \end{cases}$$

W a code book matrix, z coefficients

Gaussian:

$$p(\mathbf{z}) = \mathcal{N}(0, \sigma_z^2 \mathbf{I}) \propto \exp\left\{-\frac{1}{2\sigma_z^2} \sum_j |z_j|^2\right\}$$
$$J(\mathbf{z}) = -\ln p(\mathbf{z}|\mathbf{g}) = \|\mathbf{g} - \mathbf{HWz}\|^2 + \lambda \sum_j |z_j|^2$$

• Generalized Gaussian (sparsity,  $\beta = 1$ ):

$$p(\mathbf{z}) \propto \exp\left\{-\lambda \sum_{j} |z_{j}|^{\beta}\right\}$$
$$J(\mathbf{z}) = -\ln p(\mathbf{z}|\mathbf{g}) = \|\mathbf{g} - \mathbf{H}\mathbf{W}\mathbf{z}\|^{2} + \lambda \sum_{j} |z_{j}|^{\beta}$$

◆□ → ◆□ → ◆豆 → ◆豆 → □ 亘

► 
$$z = \arg \min_{z} \{J(z)\} \longrightarrow \hat{f} = W\hat{z}$$

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 36/56

#### Full Bayesian approach $M \cdot$

$$\mathbf{g} = \mathbf{H}\mathbf{f} + oldsymbol{\epsilon}$$

- Forward & errors model:  $\longrightarrow p(\mathbf{g}|\mathbf{f}, \boldsymbol{\theta}_1; \mathcal{M})$
- Prior models  $\longrightarrow p(\mathbf{f}|\boldsymbol{\theta}_2; \mathcal{M})$
- Hyperparameters  $\boldsymbol{\theta} = (\boldsymbol{\theta}_1, \boldsymbol{\theta}_2) \longrightarrow p(\boldsymbol{\theta} | \mathcal{M})$
- ► Bayes:  $\longrightarrow p(\mathbf{f}, \boldsymbol{\theta} | \mathbf{g}; \mathcal{M}) = \frac{p(\mathbf{g} | \mathbf{f}, \boldsymbol{\theta}; \mathcal{M}) p(\mathbf{f} | \boldsymbol{\theta}; \mathcal{M}) p(\boldsymbol{\theta} | \mathcal{M})}{p(\mathbf{g} | \mathcal{M})}$
- ► Joint MAP:  $(\widehat{\mathbf{f}}, \widehat{\boldsymbol{\theta}}) = \arg \max_{(\mathbf{f}, \boldsymbol{\theta})} \{ p(\mathbf{f}, \boldsymbol{\theta} | \mathbf{g}; \mathcal{M}) \}$
- Marginalization:  $\begin{cases} p(\mathbf{f}|\mathbf{g};\mathcal{M}) = \int p(\mathbf{f},\boldsymbol{\theta}|\mathbf{g};\mathcal{M}) \, d\mathbf{f} \\ p(\boldsymbol{\theta}|\mathbf{g};\mathcal{M}) = \int p(\mathbf{f},\boldsymbol{\theta}|\mathbf{g};\mathcal{M}) \, d\boldsymbol{\theta} \end{cases}$ ► Posterior means:  $\begin{cases} \widehat{\mathbf{f}} = \int \mathbf{f} \, p(\mathbf{f}, \boldsymbol{\theta} | \mathbf{g}; \mathcal{M}) \, \mathrm{df} \, \mathrm{d}\boldsymbol{\theta} \\ \widehat{\boldsymbol{\theta}} = \int \boldsymbol{\theta} \, p(\mathbf{f}, \boldsymbol{\theta} | \mathbf{g}; \mathcal{M}) \, \mathrm{df} \, \mathrm{d}\boldsymbol{\theta} \end{cases}$
- Evidence of the model:

$$p(\mathbf{g}|\mathcal{M}) = \iint p(\mathbf{g}|\mathbf{f}, \boldsymbol{\theta}; \mathcal{M}) p(\mathbf{f}|\boldsymbol{\theta}; \mathcal{M}) p(\boldsymbol{\theta}|\mathcal{M}) \, \mathrm{d}\mathbf{f} \, \mathrm{d}\boldsymbol{\theta}$$

A. Mohammad-Diafari. ISIP 2012. July23-28, 2012.

37/56

Two main steps in the Bayesian approach

## Prior modeling

- Separable:
  - Gaussian, Generalized Gaussian, Gamma,
  - mixture of Gaussians, mixture of Gammas, ...
- Markovian: Gauss-Markov, GGM, ...
- Separable or Markovian with hidden variables (contours, region labels)

Choice of the estimator and computational aspects

- MAP, Posterior mean, Marginal MAP
- MAP needs optimization algorithms
- Posterior mean needs integration methods
- Marginal MAP needs integration and optimization
- Approximations:
  - Gaussian approximation (Laplace)
  - Numerical exploration MCMC
  - Variational Bayes (Separable approximation)

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 38/56

# Which images I am looking for?



A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 39/56

◆□▶ ◆圖▶ ◆필▶ ◆필▶ 三回 のへで

# Which image I am looking for?



A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

40/56

# Gauss-Markov-Potts prior models for images

"In NDT applications of CT, the objects are, in general, composed of a finite number of materials, and the voxels corresponding to each materials are grouped in compact regions" How to model this prior information?



A. Mohammad-Djafari, ISIP 2012, July23-28, 2012,

41/56

ヘロト 人間ト ヘヨト ヘヨト

# Four different cases

To each pixel of the image is associated 2 variables  $f(\mathbf{r})$  and  $z(\mathbf{r})$ 

- ▶ f | z Gaussian iid, z iid : Mixture of Gaussians
- ▶ f | z Gauss-Markov, z iid : Mixture of Gauss-Markov
- ▶ f | z Gaussian iid, z Potts-Markov : Mixture of Independent Gaussians (MIG with Hidden Potts)
- ▶ f | z Markov, z Potts-Markov : Mixture of Gauss-Markov (MGM with hidden Potts)



・ロト ・ 同ト ・ ヨト ・ ヨト

A. Mohammad-Diafari. ISIP 2012. Julv23-28, 2012.

42/56

# Four different cases



# Summary of the two proposed models



**f**|**z** Gaussian iid**z** Potts-Markov

f|z Markov z Potts-Markov

(MIG with Hidden Potts) (MGM with hidden Potts)

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 44/56

# Bayesian Computation

 $p(\mathbf{f}, \mathbf{z}, \boldsymbol{\theta} | \mathbf{g}) \propto p(\mathbf{g} | \mathbf{f}, \mathbf{z}, v_{\epsilon}) \, p(\mathbf{f} | \mathbf{z}, \mathbf{m}, \mathbf{v}) \, p(\mathbf{z} | \gamma, \alpha) \, p(\boldsymbol{\theta})$ 

 $\boldsymbol{\theta} = \{ v_{\epsilon}, (\alpha_k, m_k, v_k), k = 1, \cdot, K \}$   $p(\boldsymbol{\theta})$  Conjugate priors

- Direct computation and use of  $p(\mathbf{f}, \mathbf{z}, \boldsymbol{\theta} | \mathbf{g}; \mathcal{M})$  is too complex
- Possible approximations :
  - Gauss-Laplace (Gaussian approximation)
  - Exploration (Sampling) using MCMC methods
  - Separable approximation (Variational techniques)
- Main idea in Variational Bayesian methods:

Approximate

 $p(\mathbf{f}, \mathbf{z}, \boldsymbol{ heta} | \mathbf{g}; \mathcal{M})$  by  $q(\mathbf{f}, \mathbf{z}, \boldsymbol{ heta}) = q_1(\mathbf{f}) \ q_2(\mathbf{z}) \ q_3(\boldsymbol{ heta})$ 

- Choice of approximation criterion : KL(q : p)
- Choice of appropriate families of probability laws for q<sub>1</sub>(f), q<sub>2</sub>(z) and q<sub>3</sub>(θ)

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 45/56

# MCMC based algorithm

 $p(\mathbf{f}, \mathbf{z}, \boldsymbol{\theta} | \mathbf{g}) \propto p(\mathbf{g} | \mathbf{f}, \mathbf{z}, \boldsymbol{\theta}) p(\mathbf{f} | \mathbf{z}, \boldsymbol{\theta}) p(\mathbf{z}) p(\boldsymbol{\theta})$ 

General scheme:

$$\widehat{\mathbf{f}} \sim \rho(\mathbf{f} | \widehat{\mathbf{z}}, \widehat{\boldsymbol{\theta}}, \mathbf{g}) \longrightarrow \widehat{\mathbf{z}} \sim \rho(\mathbf{z} | \widehat{\mathbf{f}}, \widehat{\boldsymbol{\theta}}, \mathbf{g}) \longrightarrow \widehat{\boldsymbol{\theta}} \sim (\boldsymbol{\theta} | \widehat{\mathbf{f}}, \widehat{\mathbf{z}}, \mathbf{g})$$

- Sample **f** from  $p(\mathbf{f}|\hat{\mathbf{z}}, \hat{\theta}, \mathbf{g}) \propto p(\mathbf{g}|\mathbf{f}, \theta) p(\mathbf{f}|\hat{\mathbf{z}}, \hat{\theta})$ Needs optimisation of a quadratic criterion.
- Sample z from p(z|f, θ, g) ∝ p(g|f, z, θ) p(z) Needs sampling of a Potts Markov field.
- ► Sample  $\theta$  from  $p(\theta | \hat{\mathbf{f}}, \hat{\mathbf{z}}, \mathbf{g}) \propto p(\mathbf{g} | \hat{\mathbf{f}}, \sigma_{\epsilon}^2 \mathbf{I}) p(\hat{\mathbf{f}} | \hat{\mathbf{z}}, (m_k, v_k)) p(\theta)$ Conjugate priors  $\longrightarrow$  analytical expressions.

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 46/56

# Application of CT in NDT

Reconstruction from only 2 projections

$$g_1(x) = \int f(x, y) \, dy$$
$$g_2(y) = \int f(x, y) \, dx$$

- Given the marginals  $g_1(x)$  and  $g_2(y)$  find the joint distribution f(x, y).
- ► Infinite number of solutions :  $f(x, y) = g_1(x) g_2(y) \Omega(x, y)$  $\Omega(x, y)$  is a Copula:

$$\int \Omega(x,y) \, \mathrm{d}x = 1 \quad \text{and} \quad \int \Omega(x,y) \, \mathrm{d}y = 1$$

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 47/56

# Application in CT



flz g|f Ζ  $q(\mathbf{r}) \in \{0,1\}$  $\mathbf{g} = \mathbf{H}\mathbf{f} + \boldsymbol{\epsilon}$ iid Gaussian iid  $\mathbf{g} | \mathbf{f} \sim \mathcal{N}(\mathbf{H}\mathbf{f}, \sigma_{\epsilon}^2 \mathbf{I})$  $1 - \delta(z(\mathbf{r}) - z(\mathbf{r}'))$ or or Gaussian Gauss-Markov binary Potts Forward model Gauss-Markov-Potts Prior Model Auxilary Unsupervised Bayesian estimation:

 $p(\mathbf{f}, \mathbf{z}, \boldsymbol{\theta} | \mathbf{g}) \propto p(\mathbf{g} | \mathbf{f}, \mathbf{z}, \boldsymbol{\theta}) p(\mathbf{f} | \mathbf{z}, \boldsymbol{\theta}) p(\boldsymbol{\theta})$ 

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 4

48/56

・ロト ・ 日 ・ ・ 日 ・ ・ 日 ・

# Results: 2D case



A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

49/56

# Some results in 3D case

(Results obtained with collaboration with CEA)



#### M. Defrise



FeldKamp



Proposed method

<ロト < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < 回 > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > < □ > <

A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

2, 50/56

# Some results in 3D case



A. Mohammad-Djafari,

ISIP 2012, July23-28, 2012,

2, 51/56

ロト (四) (三) (三) (三) (三) (三) (三)

# Some results in 3D case



A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 52/56

# Application: liquid evaporation in metalic esponge



A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 53/56

・ロト・西ト・モディ 明・ うくぐ

# Conclusions

- Gauss-Markov-Potts are useful prior models for images incorporating regions and contours
- Bayesian computation needs often pproximations (Laplace, MCMC, Variational Bayes)
- Application in different CT systems (X ray, Ultrasound, Microwave, PET, SPECT) as well as other inverse problems

Work in Progress and Perspectives :

- Efficient implementation in 2D and 3D cases using GPU
- Evaluation of performances and comparison with MCMC methods
- Application to other linear and non linear inverse problems: (PET, SPECT or ultrasound and microwave imaging)

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 54/56

# Some references

- A. Mohammad-Djafari (Ed.) Problèmes inverses en imagerie et en vision (Vol. 1 et 2), Hermes-Lavoisier, Traité Signal et Image, IC2, 2009,
- A. Mohammad-Djafari (Ed.) Inverse Problems in Vision and 3D Tomography, ISTE, Wiley and sons, ISBN: 9781848211728, December 2009, Hardback, 480 pp.
- H. Ayasso and Ali Mohammad-Djafari Joint NDT Image Restoration and Segmentation using Gauss-Markov-Potts Prior Models and Variational Bayesian Computation, To appear in IEEE Trans. on Image Processing, TIP-04815-2009.R2, 2010.
- H. Ayasso, B. Duchene and A. Mohammad-Djafari, Bayesian Inversion for Optical Diffraction Tomography Journal of Modern Optics, 2008.
- A. Mohammad-Djafari, Gauss-Markov-Potts Priors for Images in Computer Tomography Resulting to Joint Optimal Reconstruction and segmentation, International Journal of Tomography & Statistics 11: W09. 76-92, 2008.
- A Mohammad-Djafari, Super-Resolution : A short review, a new method based on hidden Markov modeling of HR image and future challenges, The Computer Journal doi:10,1093/comjnl/bxn005:, 2008.
- O. Féron, B. Duchène and A. Mohammad-Djafari, Microwave imaging of inhomogeneous objects made of a finite number of dielectric and conductive materials from experimental data, Inverse Problems, 21(6):95-115, Dec 2005.
- M. Ichir and A. Mohammad-Djafari, Hilden markov models for blind source separation, IEEE Trans. on Signal Processing, 15(7):1887-1899, Jul 2006.
- F. Humblot and A. Mohammad-Djafari, Super-Resolution using Hidden Markov Model and Bayesian Detection Estimation Framework, EURASIP Journal on Applied Signal Processing, Special number on Super-Resolution Imaging: Analysis, Algorithms, and Applications:ID 36971, 16 pages, 2006.

#### O. Féron and A. Mohammad-Djafari, Image fusion and joint segmentation using an MCMC algorithm, Journal of Electronic Imaging, 14(2):paper no. 023014, Apr 2005.

- H. Snoussi and A. Mohammad-Djafari, Fast joint separation and segmentation of mixed images, Journal of Electronic Imaging, 13(2):349-361, April 2004.
- A. Mohammad-Djafari, J.F. Giovannelli, G. Demoment and J. Idier, Regularization, maximum entropy and probabilistic methods in mass spectrometry data processing problems, Int. Journal of Mass Spectrometry, 215(1-3):175-193, April 2002.

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 55/56

# Thanks, Questions and Discussions

#### Thanks to:

My graduated PhD students:

- H. Snoussi, M. Ichir, (Sources separation)
- F. Humblot (Super-resolution)
- H. Carfantan, O. Féron (Microwave Tomography)
- S. Fékih-Salem (3D X ray Tomography)

#### My present PhD students:

- H. Ayasso (Optical Tomography, Variational Bayes)
- D. Pougaza (Tomography and Copula)

D. Fall (Emission Positon Tomography, Non Parametric Bayesian)

#### My colleages in GPI (L2S) & collaborators in other instituts:

- B. Duchêne & A. Joisel (Inverse scattering and Microwave Imaging)
- N. Gac & A. Rabanal (GPU Implementation)
- Th. Rodet (Tomography)
- ▶ \_\_\_
- A. Vabre & S. Legoupil (CEA-LIST), (3D X ray Tomography)
- E. Barat (CEA-LIST) (Positon Emission Tomography, Non Parametric Bayesian)

C. Comtat (SHFJ, CEA)(PET, Spatio-Temporal Brain activity)

## **Questions and Discussions**

A. Mohammad-Djafari, ISIP 2012, July23-28, 2012, 56/56

Sh. Zhu (SAR Imaging)