Bayesian Microwave Breast Imaging

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Summary



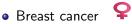
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- Inversion
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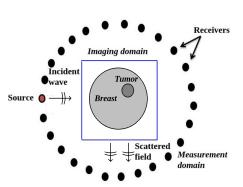
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Motivation



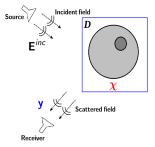
- Most commonly diagnosed cancer
- $\bullet\,$ Second cause of cancer death for women \to Need to early stage cancer detection
- Detection techniques
 - X-ray mammography: Ionizing radiation, costly, high false-positive rate, low sensitivity
 - Ultrasound and MRI: High spatial resolution but luck of functional information
 - Microwave imaging: non negligible dielectric contrast between cancerous and normal healthy breast tissues, non-ionizing nature, easy accessibility \rightarrow Promising alternative for breast tumor detection

Microwave imaging



- Different source positions
- Several receivers and frequencies in the microwave range
- Retrieve unknown target (electrical permittivity and conductivity) from measurements of the scattered field, the incident wave being known
- Non-linear ill-posed inverse problem

Domain integral representation



Observation equation

$$\mathbf{y}(\mathbf{r}) = k_1^2 \int_{\mathcal{D}} G(\mathbf{r}, \mathbf{r}') \, \chi(\mathbf{r}') E(\mathbf{r}) \, \mathrm{d}\mathbf{r}'$$

• Coupling equation $E(\mathbf{r}) = E^{inc}(\mathbf{r}) + k_1^2 \int_{\mathcal{D}} G(\mathbf{r}, \mathbf{r}') \chi(\mathbf{r}') E(\mathbf{r}) d\mathbf{r}'$

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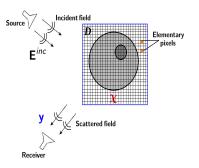
• *E*(**r**): total field in the object

• $\chi(\mathbf{r}) = (k(\mathbf{r})^2 - k_1^2)/k_1^2$: normalized contrast function

- $k(\mathbf{r})^2 = \omega^2 \epsilon_0 \mu_0 \frac{\epsilon_r(\mathbf{r})}{\epsilon_r(\mathbf{r})} + i\omega \mu_0 \sigma(\mathbf{r}), k_1 = \text{propagation constant of the outside medium}$
- $G(\mathbf{r}, \mathbf{r}')$: Green's function

Discretized model

- Test domain \mathcal{D} partitioned into $N_{\mathcal{D}}$ elementary pixels
- Coupling equation rewritten in terms of contrast sources:
 w(r') = χ(r')E(r')
- Method of moments [Harrington, 1993]
- \Rightarrow bilinear discret model:
- $\begin{cases} \mathbf{y} = \mathbf{G}^{\circ} \mathbf{w} + \epsilon \text{ (observation)} \\ \mathbf{w} = \boldsymbol{\chi} \mathbf{E}^{inc} + \boldsymbol{\chi} \mathbf{G}^{c} \mathbf{w} + \boldsymbol{\xi} \text{ (coupling)} \end{cases}$
- $\epsilon, \pmb{\xi}$: model and measurements errors



Bayesian framework

$$\begin{cases} \mathbf{y} = \mathbf{G}^{\circ} \mathbf{w} + \epsilon \text{ (observation)} \\ \mathbf{w} = \mathbf{\chi} \mathbf{E}^{inc} + \mathbf{\chi} \mathbf{G}^{c} \mathbf{w} + \boldsymbol{\xi} \text{ (coupling)} \end{cases}$$

Let consider the first equation:

$$\mathbf{y} = \mathbf{G}^{o}\mathbf{w} + \boldsymbol{\epsilon}, \quad p(\boldsymbol{\epsilon}) = \mathcal{N}(\boldsymbol{\epsilon}|\mathbf{0}, \sigma_{\epsilon}^{2}\mathbf{I})$$

Bayes rule:

$$p(\mathbf{y}|\mathbf{w}) = \frac{p(\mathbf{y}|\mathbf{w})p(\mathbf{w})}{p(\mathbf{y})}$$

$$\begin{cases} p(\mathbf{y}|\mathbf{w}) = \mathcal{N}(\mathbf{y}|\mathbf{G}^{\circ}\mathbf{w}, \sigma_{\epsilon}^{2}\mathbf{I}) \\ p(\mathbf{w}) = \mathcal{N}(\mathbf{w}|0, \sigma_{w}^{2}\mathbf{I}) \end{cases} \rightarrow p(\mathbf{w}|\mathbf{y}) = \mathcal{N}(\mathbf{w}|\widehat{\mathbf{w}}, \widehat{\mathbf{\Sigma}})$$

$$\begin{cases} \widehat{\mathbf{w}} = [\mathbf{G}^{\circ^{T}}\mathbf{G}^{\circ} + \lambda\mathbf{I}]^{-1}\mathbf{G}^{\circ^{T}}\mathbf{y} \\ \widehat{\mathbf{\Sigma}} = [\mathbf{G}^{\circ}\mathbf{G}^{\circ} + \lambda\mathbf{I}]^{-1} \end{cases}$$

We can do the same with the second equation.

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Bayesian framework

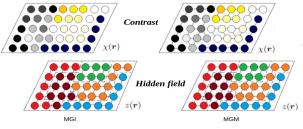
$$p(\boldsymbol{\chi}, \boldsymbol{w}, \boldsymbol{\Theta} | \boldsymbol{y}; \mathcal{M}) = \frac{p(\boldsymbol{y} | \boldsymbol{w}, \boldsymbol{\Theta}; \mathcal{M}) p(\boldsymbol{w} | \boldsymbol{\chi}, \boldsymbol{\Theta}; \mathcal{M}) p(\boldsymbol{\chi} | \boldsymbol{\Theta}; \mathcal{M}) p(\boldsymbol{\Theta} | \mathcal{M})}{p(\boldsymbol{y} | \mathcal{M})}$$

- ⊖: hyper-parameters
- $p(\mathbf{y}|\mathbf{w}, \Theta; \mathcal{M})$ (observation equation)
- $p(\mathbf{w}|\boldsymbol{\chi}, \Theta; \mathcal{M})$ (coupling equation)
- $p(\chi | \Theta; \mathcal{M})$: a priori on the object
- $p(\Theta|\mathcal{M})$: a priori information on the hyperparameters
- $p(\boldsymbol{\chi}, \boldsymbol{w}, \boldsymbol{\Theta} | \boldsymbol{y}; \mathcal{M})$: a posteriori

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Gauss-Markov-Potts prior

• Objects composed of a finite number *K* of materials distributed into homogenous and compact regions



 $p(\chi(\mathbf{r})|z(\mathbf{r})) = \mathcal{N}(m_k(\mathbf{r}), v_k(\mathbf{r})), \ p(\mathbf{z}|\lambda) = Potts \ model$

- Mixture of independant Gaussian laws (MGI): pixels of the same class are assumed independant
- Gauss-Markov mixture model (MGM): a high correlation between pixels of the same class by means of a Markov field

Gauss-Markov-Potts prior

• Homogeneity of a class:

$$p(\chi(\mathbf{r})|z(\mathbf{r})) = \mathcal{N}(m_k(\mathbf{r}), v_k(\mathbf{r})), \qquad k = 1, \dots, K,$$

$$\begin{aligned} - v_k(\mathbf{r}) &= v_k \quad \forall \mathbf{r} \in \mathcal{R}_k \\ - m_k(\mathbf{r}) &= \begin{cases} m_k & \text{if } \mathcal{C}(\mathbf{r}) = 1 \\ \frac{1}{N_{\mathcal{V}}} \sum_{\mathbf{r}' \in \mathcal{V}(\mathbf{r})} \chi(\mathbf{r}') & \text{if } \mathcal{C}(\mathbf{r}) = 0, \\ \mathcal{C}(\mathbf{r}) &= 1 - \prod_{\mathbf{r}' \in \mathcal{V}(\mathbf{r})} \delta(z(\mathbf{r}') - z(\mathbf{r})), \ \mathcal{V}(\mathbf{r}) \text{ is a neighborhood of } \mathbf{r} \end{cases} \end{aligned}$$

made of the four nearest pixels and $N_{\mathcal{V}} = card(\mathcal{V})$.

• Compactness of the regions (Potts):

$$p(\mathbf{z}|\lambda) \propto \exp\left[\sum_{\mathbf{r} \in \mathcal{D}} \left(\Phi(z(\mathbf{r})) + \frac{\lambda}{2} \sum_{\mathbf{r}' \in \mathcal{V}(\mathbf{r})} \delta\left(z(\mathbf{r}) - z(\mathbf{r}')\right)\right)\right]$$

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Probabilistic modeling

• Model and measurement errors:

$$\boldsymbol{\epsilon} \sim \mathcal{N}(\mathbf{0}, \mathbf{v}_{\epsilon} \mathbf{I}), \;\; \boldsymbol{\xi} \sim \mathcal{N}(\mathbf{0}, \mathbf{v}_{\xi} \mathbf{I})$$

Hyperparameters:

$$p(m_k) = \mathcal{N}(\mu, \tau), \quad p(v_k) = \mathcal{IG}(\eta, \phi)$$

$$p(v_{\epsilon}) = \mathcal{IG}(\eta_{\epsilon}, \phi_{\epsilon}), \quad p(v_{\xi}) = \mathcal{IG}(\eta_{\xi}, \phi_{\xi})$$

• <u>A posteriori:</u>

 $p(\boldsymbol{\chi}, \mathbf{w}, \mathbf{z}, \boldsymbol{\Theta} | \mathbf{y}) \propto p(\mathbf{y} | \mathbf{w}, v_{\epsilon}) p(\mathbf{w} | \boldsymbol{\chi}, v_{\xi}) p(\boldsymbol{\chi} | \mathbf{z}, \mathbf{m}, \mathbf{v})$ $\times p(\mathbf{z} | \lambda) p(\mathbf{m} | \mu, \tau) p(\mathbf{v} | \eta, \phi)$ $\times p(v_{\epsilon} | \eta_{\epsilon}, \phi_{\epsilon}) p(v_{\xi} | \eta_{\xi}, \phi_{\xi})$

with $\Theta = \{\mathbf{m}, \mathbf{v}, v_{\epsilon}, v_{\xi}\}.$

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Bayesian inversion techniques

$$p(\boldsymbol{\chi}, \mathbf{w}, \mathbf{z}, \Theta | \mathbf{y}) \propto p(\mathbf{y} | \mathbf{w}, v_{\epsilon}) p(\mathbf{w} | \boldsymbol{\chi}, v_{\xi}) p(\boldsymbol{\chi} | \mathbf{z}, \mathbf{m}, \mathbf{v})$$

$$\times p(\mathbf{z} | \lambda) p(\mathbf{m} | \mu, \tau) p(\mathbf{v} | \eta, \phi)$$

$$\times p(v_{\epsilon} | \eta_{\epsilon}, \phi_{\epsilon}) p(v_{\xi} | \eta_{\xi}, \phi_{\xi})$$

- Joint Maximum A Posteriori (JMAP) (intractable solutions in non-linear cases) [Gharsalli et al., 2014]
 → needs to approximate the joint *a posteriori* distribution
- Monte-Carlo Markov Chain sampling (MCMC) (costly) [Féron, 2006]
- Variational Bayesian Approach (VBA) (less costly alternative) [Ayasso et al., 2012]

Variational Bayesian Approach (VBA) [Mackay, 2003]

Aim:

Approximating $p(\boldsymbol{\chi}, \mathbf{w}, \mathbf{z}, \Theta | \mathbf{y}; \mathcal{M})$ by a separable law:

$$q({oldsymbol \chi}, {oldsymbol w}, {oldsymbol z}, \Theta) = q_1({oldsymbol \chi})q_2({oldsymbol w})q_3({oldsymbol z})q_4(\Theta)$$

• Criterion:
$$KL(\mathbf{q} : \mathbf{p}) = \int \mathbf{q} \ln \frac{\mathbf{q}}{\mathbf{p}} = \left\langle \frac{\mathbf{q}}{\mathbf{p}} \right\rangle_{\mathbf{q}} = \mathcal{F}(\mathbf{q}) + \ln p(\mathbf{y}|\mathcal{M})$$

Free negative energy:
$$\mathcal{F}(\mathbf{q}) = \left\langle \ln \frac{P(\mathbf{u}, \mathbf{y}|\mathcal{M})}{q(\mathbf{u})} \right\rangle_{\mathbf{q}}, \ \mathbf{u} = \{ \boldsymbol{\chi}, \mathbf{w}, \mathbf{z}, \Theta \}$$

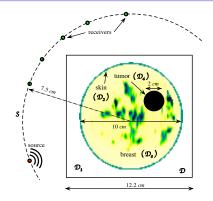
• Minimize $\mathsf{KL}(\mathbf{q}:\mathbf{p}) \Leftrightarrow \mathsf{Maximize}\ \mathcal{F}(\mathbf{q})$

• Find:
$$\mathbf{q}^{opt} = \arg \max_{\mathbf{q}} \mathcal{F}(\mathbf{q})$$

•
$$q(\mathbf{u}_i) \propto \exp\left\{\langle \log(p(\mathbf{u}, \mathbf{y})) \rangle_{\prod_{j \neq i} q(\mathbf{u}_j)} \right\}$$

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Measurement configuration: application to breast cancer detection



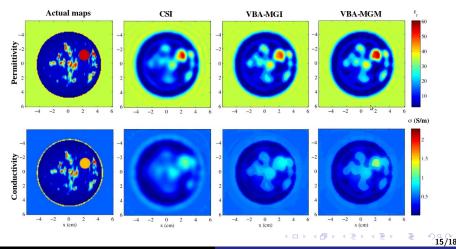
- Breast model built up from MRI scan
 Zastrew and Hagness 2009
 - [Zastrow and Hagness, 2008]

- 64 sources
- 64 receivers
- 6 frequencies in the band 0.5 3 GHz

$\mathcal{D} = N_x \times N_y$	D1 ($\epsilon_1, \sigma_1(S/m)$)	D2 ($\epsilon_2, \sigma_2(S/m)$)	D3 ($\epsilon_3, \sigma_3(S/m)$)	D4 ($\epsilon_3, \sigma_3(S/m)$)
120 imes 120	(10, 0.5)	(6.12, 0.11)	([2.46, 60.6], [0.01, 2.28])	(55.3, 1.57)

Reconstruction

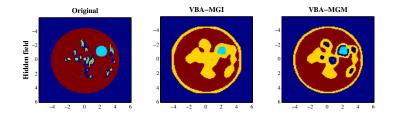
CSI: Contrast Source Inversion, VBA: Variational Bayesian Approach, MGI: Independent Gaussian mixture, MGM: Gauss-Markov mixture



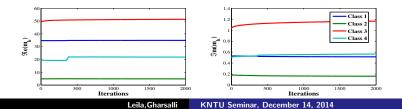
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Reconstruction



– 3267 and 3029 pixels have undergone a change of class during the iterative process



Conclusions :

- Bayesian approach to microwave imaging: complexity of breast imaging compared to previous applications [Ayasso, 2010]

- Better resolution with VBA than with CSI
- Better identication of heterogeneous areas with MGM than with MGI prior
- Risk of hiding small details of interest

Prospects

- Accelerate the convergence by introducing a gradient step
- Account for breast tissue frequency dispersivity by means of Debye models
- Test on laboratory controlled experimental data involving breast phantoms

- Study the false alarm rate of the method \rightarrow need of a reference database



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Thanks!

Questions?

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